

Production of ^{44m}Sc for multiple-isotope PET

T. Fukuchi,*¹ S. Yano,*² H. Haba,*¹ and Y. Watanabe*¹

We have been working toward the development of a next-generation positron emission tomography (PET) system, known as multiple-isotope PET (MI-PET). MI-PET is designed to coincide with γ -ray using additional detectors and identify the tracer by detecting the prompt γ -ray, which is emitted after positron emission from positron- γ emitter. Figure 1 shows an image and schematic illustration of the developed MI-PET system. The system is composed of a PET system and additional γ -ray detectors. The PET system consists of pixelized gadolinium orthosilicate (GSO) scintillation detectors and has a ring geometry with an inner diameter and width of 95 mm and 37.5 mm, respectively. Eight bismuth germanium oxide (BGO) scintillation detectors constitute the additional eight detectors, each with a dimension of $50 \times 50 \times 30 \text{ mm}^3$, arranged in two rings mounted on each side of the PET ring.¹⁾

For multiple-isotope imaging using MI-PET, at least one positron- γ emitter is necessary as a tracer. Scandium-44 is one of the candidates for the specific radioactive tracer for MI-PET owing to its large positron and γ -ray emission ratio and moderate half-life (^{44}Sc : 3.97 h, ^{44m}Sc : 58.61 h). Therefore, we studied the production of ^{44m}Sc and its imaging using MI-PET.

For ^{44m}Sc production, we used $^{\text{nat}}\text{CaO}$ powder as the target material, which was pressed into a disk with an inner diameter and thickness of 10-mm and $376\text{-mg}/\text{cm}^2$, respectively. The target was irradiated for 3 h with a 24-MeV deuteron beam having an intensity of $3.0 \mu\text{A}$ at the RIKEN AVF cyclotron. The irradiated CaO target was dissolved in 6 M HCl and evaporated to become dry. Subsequently, the residue was dissolved in 5 mL of 2 M HCl. The solution was passed through an anion exchange resin column (DGA resin, particle size: 50–100 μm) filled in a Muromac column.²⁾ The resin was then washed with 5 mL of 2 M HCl and ^{44m}Sc was eluted from the resin with 10 mL of 0.1 M HCl. Finally, approximately 2.0 MBq of ^{44m}Sc with 90% radiochemical

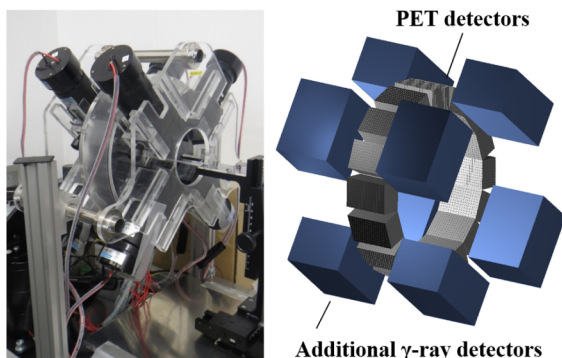


Fig. 1. Image (left) and schematic illustration (right) of the developed PET system.

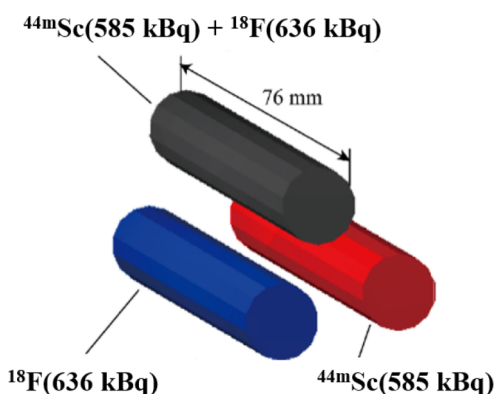


Fig. 2. Illustration of rod phantom configuration.

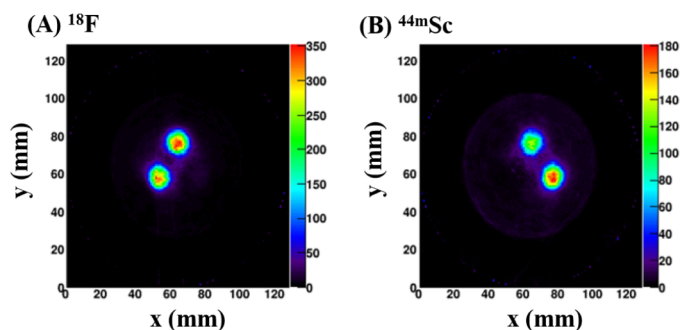


Fig. 3. The x-y plane projection images of rod phantom. Images were reconstructed with (A) absence or (B) presence of γ -ray detection.

yield was obtained.

To test the imaging ability of the MI-PET system for ^{44m}Sc , we scanned a dual radionuclide rod phantom that comprised three cylindrical rods with a diameter and length of 10 mm and 76 mm, respectively. Scandium-44m and ^{18}F (pure positron emitter) dissolved in water were poured into the rods. The first rod had ^{44m}Sc (585 kBq) and ^{18}F (636 kBq) activities. The second and third rods had ^{44m}Sc (585 kBq) and ^{18}F (636 kBq) activities, respectively. The configuration of this rod phantom is illustrated in Fig. 2. The rods were positioned parallel to the scanner's axial direction and a 30-min scan was performed.

Figure 3 shows the reconstructed phantom images as the x-y plane projection images of the rod phantom with the absence (A) or presence (B) of γ -ray detection. From these images, the distribution of ^{44m}Sc and ^{18}F is evident.

This study demonstrates the feasibility of ^{44m}Sc imaging using MI-PET. In future, we will conduct multiple isotope animal experiments using ^{44m}Sc and the other PET tracer. We will also synthesize useful MI-PET drug labeled with ^{44m}Sc .

References

- 1) T. Fukuchi *et al.*, *Med. Phys.* **40**, 6, 2257 (2017).
- 2) C. Alliot *et al.*, *Nucl. Med. Bio.* **42**, 524 (2015).

*¹ RIKEN Center for Biosystems Dynamics Research

*² RIKEN Nishina Center